

*Supporting Information for*

# Regulation of Drug Release by Tuning Surface Textures of Biodegradable Polymer Microparticles

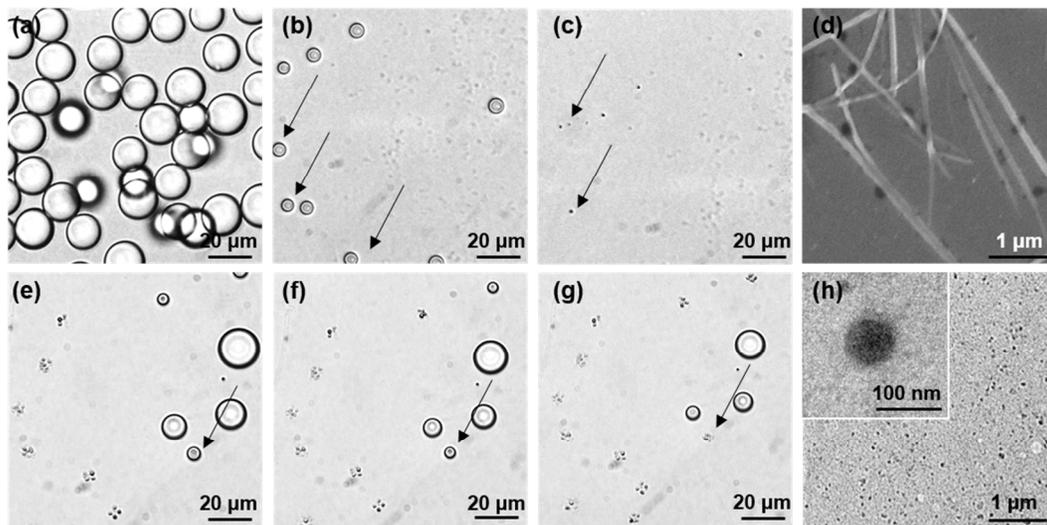
*Mubashir Hussain,<sup>#</sup> Jun Xie,<sup>#</sup> Zaiyan Hou, Khurram Shezad, Jiangping Xu, Ke Wang, Yujie Gao,  
Lei Shen, and Jintao Zhu\**

Key Laboratory of Materials Chemistry for Energy Conversion and Storage (HUST), Ministry of Education, School of Chemistry and Chemical Engineering, Huazhong University of Science and Technology, Wuhan 430074, China

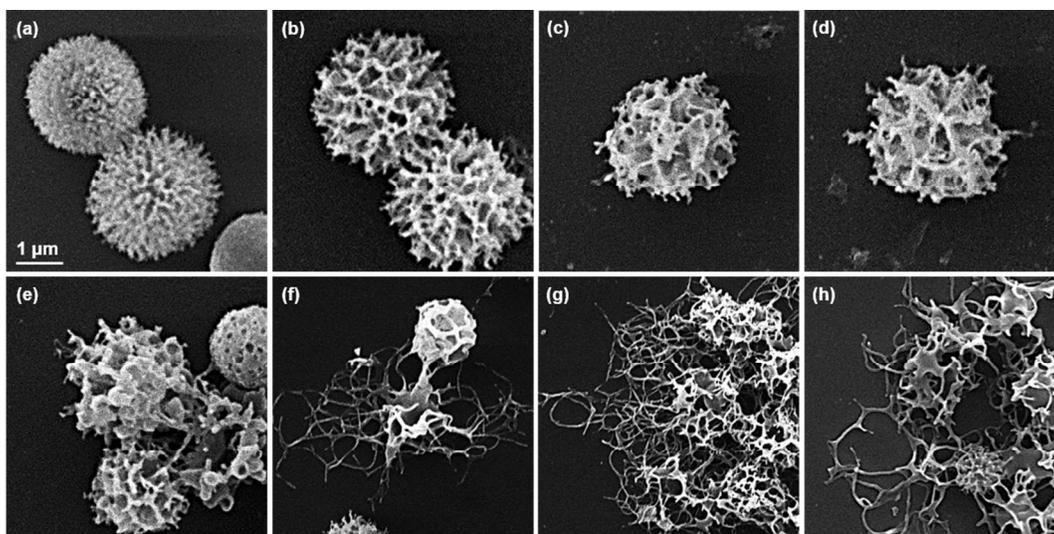
<sup>#</sup> These authors contribute equally to this work

\*Corresponding author. E-mail: [jtzhu@mail.hust.edu.cn](mailto:jtzhu@mail.hust.edu.cn)

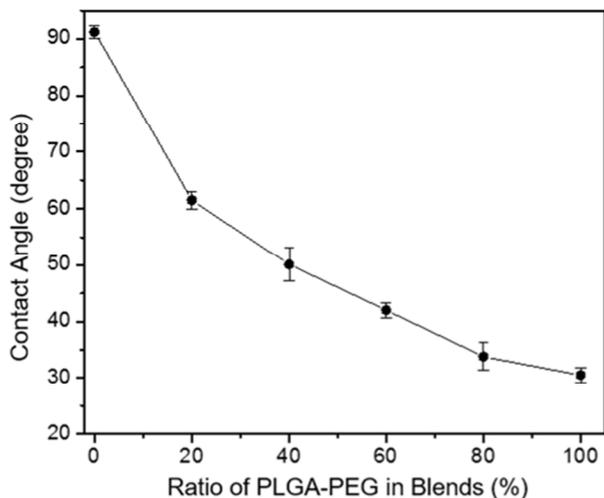
**Supporting figures:**



**Figure S1.** Optical microscopy images for the evolution of emulsion droplets containing: (a-c) PLGA<sub>5k</sub>-*b*-PEG<sub>5k</sub> and (e-g) PLGA<sub>10k</sub>-*b*-PEG<sub>20k</sub>. 10 mg/mL polymers were dissolved in DCM. The droplets shrank first, and then break into tiny droplets. Arrows show the shrinkage and breakage of the emulsion droplets. (d) is the representative SEM image showing the wormlike micelles obtained from PLGA<sub>5k</sub>-*b*-PEG<sub>5k</sub> while (h) is the bright field TEM image showing the spherical micelles obtained from PLGA<sub>10k</sub>-*b*-PEG<sub>20k</sub>. Inset in image (d) is the magnified TEM image for a spherical micelle.

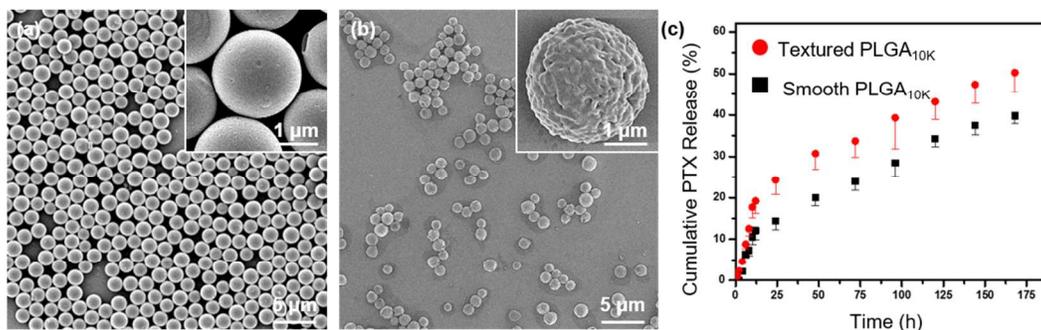


**Figure S2.** SEM images of the assemblies obtained from the binary blends of PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub> with PLGA<sub>10k</sub>-*b*-PEG<sub>20k</sub>. The total polymer concentration of the blends was same (10 mg/mL) in all cases while the ratio of PLGA<sub>10k</sub>-*b*-PEG<sub>20k</sub> in the blends was: (a) 10%, (b) 20%, (c) 30%, (d) 40%, (e) 50%, (f) 60%, (g) 70% and (h) 80%. (a-e) Roughness of the microparticles increased when increasing the ratio of PLGA<sub>10k</sub>-*b*-PEG<sub>20k</sub> in the blends up to 50%. Further increase of PLGA<sub>10k</sub>-PEG<sub>20k</sub> causes qualitatively different interfacial instability in the system and leads to the formation of polymer micelles (f-h). Scale bar shown in (a) applies to all other images.



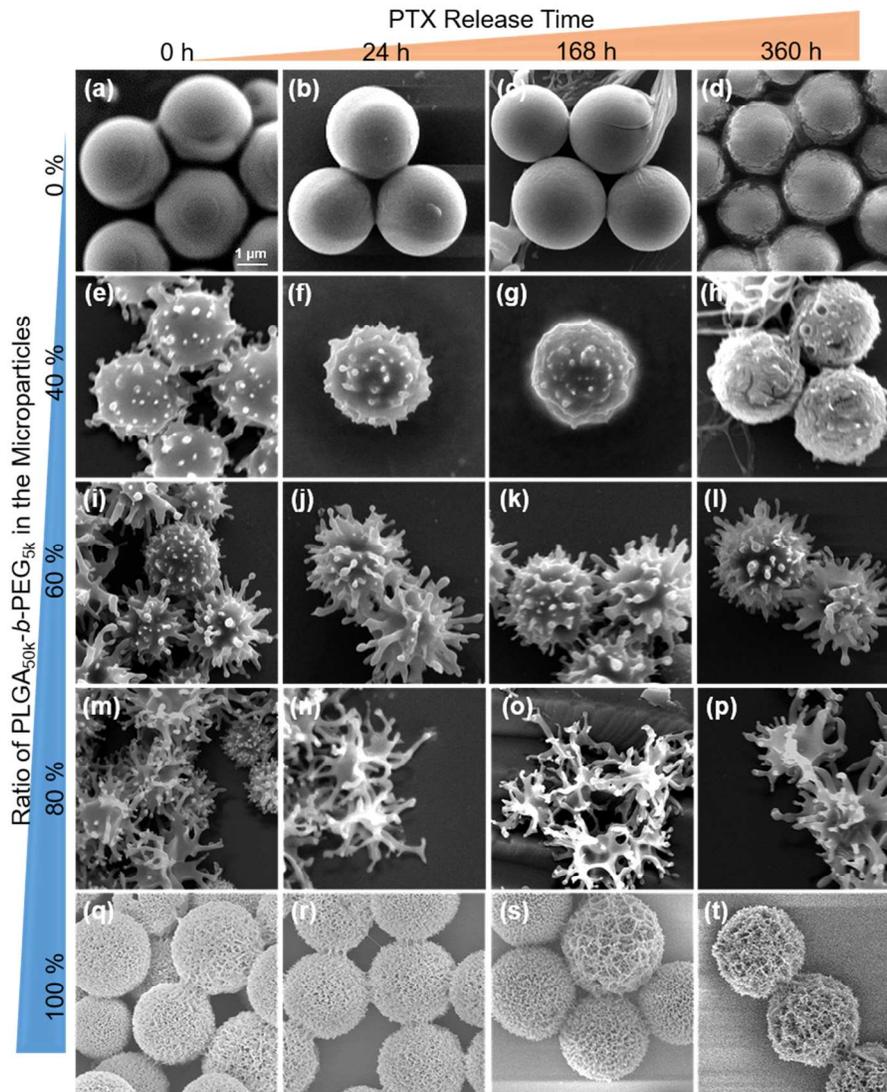
**Figure S3.** Plot shows the water contact angle on films of PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub>/PLGA<sub>100k</sub> blended microparticles. Clearly, contact angle decreases with the increase of PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub> in the polymer blends, indicating that the hydrophilicity of the polymer particles increase with the increase of surface area. Error bar represents the standard deviation.

We note that water contact angle usually increases with the increase of surface area.<sup>1-2</sup> However, in this case, with the increase of the surface area, component of the polymers will change since we used polymer blends. In general, as the PLGA-*b*-PEG content increase in the blends of PLGA-*b*-PEG/PLGA, the hydrophilic content will increase and the surface rough will enlarge (Figure 3). With the increase of surface area (roughness), more hydrophilic component (*e.g.*, PEG) will expose on the surface of the particles, resulting in the increase of the hydrophilicity.

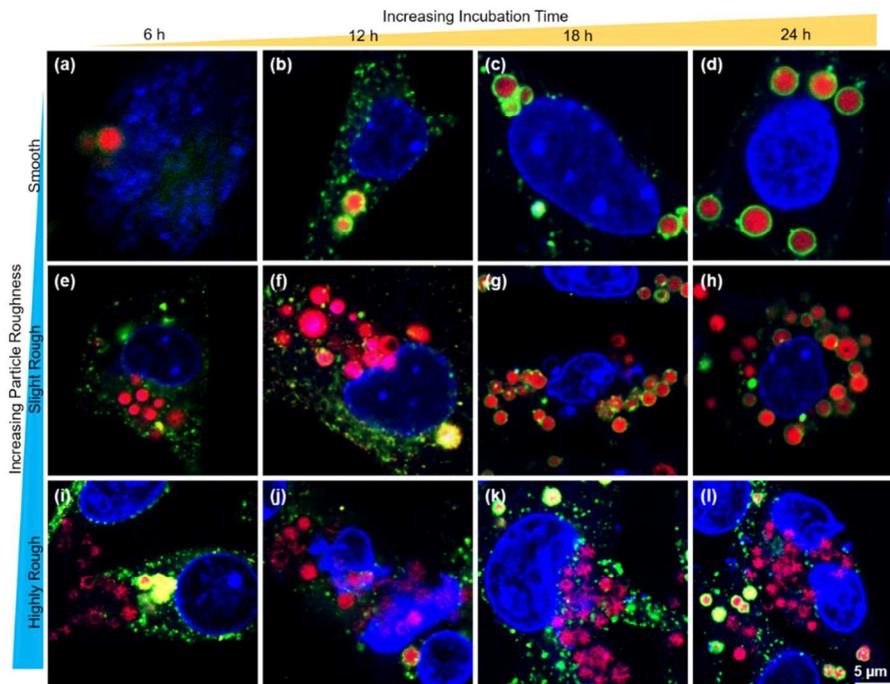


**Figure S4.** SEM images of PTX loaded (a) smooth and (b) textured PLGA<sub>10k</sub> microparticles. (c) Plot shows the PTX release profile for the PTX-poaded smooth and textured PLGA particles. Clearly, textured particles demonstrate enhanced drug release compared to the smooth ones.

Smooth PTX-loaded PLGA<sub>10k</sub> microparticles were produced in the same procedure, as decribed in the text. To produce the rough PLGA<sub>10k</sub> microparticles, PLGA<sub>10k</sub> and PTX (weight ratio of PLGA<sub>10k</sub>/PTX 10:1) were dissolved in DCM. 3 mg n-hexadecanol (HD, acting as a co-surfactant) was added to the above PLGA<sub>10k</sub>/PTX solution. The resulting solution was then emulsified with SDS (5 mg/mL) aqueous solution through microfluidic technique, as described in the text. The formed emulsion droplets were allowed in the evaporation device. Upon solvent extraction, the emulsion droplets changed their morphologies as a result of vanished interfacial tension with the assistance of added HD.<sup>1</sup> After complete removal of organic solvent, polymer microparticles with textured surfaces were obtained.



**Figure S5.** SEM images of the PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub>/PLGA<sub>100k</sub> polymer microparticles with different PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub> ratios at various period of drug release. Clearly, surface morphology of the polymer particles did not significantly change during the period of drug release investigation, indicating that the drug release pattern is a diffusion controlled mode. The scale bar in (a) applies to all other images.



**Figure S6.** CLSM images showing the cellular uptake of Nile Red labelled smooth (a-d), slight rough (e-h) and highly rough (i-l) polymer microparticles by B16-F10 melanoma cell for (a, e, i) 6h, (b, f, j) 12h, (c, g, k) 18h and (d, h, l) 24 h, respectively. Cell lysosomes were stained with Lyso Tracker Green DND-26 (green) while blue Hoechst was used to label the nuclei. The microparticles in images (a-d) are the smooth (Neat PLGA<sub>100k</sub>), (e-h) slightly rough (PLGA<sub>100k</sub>/PLGA<sub>50k</sub>-b-PLGA<sub>5k</sub>=60:40) and (i-l) are highly rough (PLGA<sub>100k</sub>/PLGA<sub>50k</sub>-b-PLGA<sub>5k</sub>=20:80). The microparticles were co-cultured with cells in well plates and imaged after a given time period. The scale bar in image (l) can be applied to all other images.

Clearly, the polymer microparticles can be observed inside the B16-F10 cells, indicating that the microparticles are uptaken by the cancer cells, and the microparticles can act as drug carriers to successfully transport hydrophobic drugs to the cancer cells.

### Supporting movies:

**Movie 1.** Real-time evolution of the emulsion droplets containing neat PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub> as DCM evaporates. During the extraction of solvent, the droplets shrink and then expand. Tiny protrusions start to appear due to the interfacial instability, and finally yielding particles with rough surface.

**Movie 2.** Real-time evolution of the emulsion droplets containing neat PLGA<sub>5k</sub>-*b*-PEG<sub>5k</sub> as DCM evaporates. During the extraction of solvent, the droplets shrink and then break into tiny droplets, finally disappearing in the aqueous phase.

**Movie 3.** Real-time evolution of the emulsion droplets containing binary blends of PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub>/PLGA<sub>100k</sub> with PLGA<sub>50k</sub>-*b*-PEG<sub>5k</sub> content of 70% as DCM evaporates. The emulsion droplets shrink first and then expand. Spiky and rough surfaces start to appear. Morphology of the droplets is finally frozen, and microparticles with highly rough surfaces are observed.

**Movie 4.** Real-time evolution of emulsion droplets containing PLGA<sub>10k</sub> in DCM. 3 mg HD was added to the oil phase to lower the oil/water interfacial tension. During the process of solvent evaporation, the emulsion droplets change their morphologies a little under optical microscopy investigation and give rise to the formation of textured microparticles.

### References:

- (1) Liu, S.; Deng, R.; Li, W.; Zhu, J. Polymer Microparticles with Controllable Surface Textures Generated through Interfacial Instabilities of Emulsion Droplets. *Adv. Funct. Mater.* **2012**, *22*, 1692-1697.
- (2) Wenzel, R. N. Resistance of Solid Surfaces to Wetting by Water. *Ind. Eng. Chem.* **1936**, *28*, 988-994.