

## Supporting information

### **A unique sensing interface that allows the development of an electrochemical immunosensor for the detection of Tumor Necrosis Factor $\alpha$ in whole blood**

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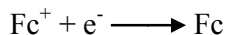
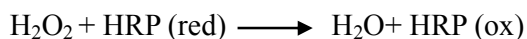
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**Electrochemical Response to Hydrogen Peroxide at the Immunosensor.** The electrocatalytic reactivity of the final immunosensor towards  $\text{H}_2\text{O}_2$  was investigated by cyclic voltammetry. Figure. S-1(a) depicts the current response in the absence and presence of  $\text{H}_2\text{O}_2$ . A pair of redox peaks were observed in the blank substrate solution, which contributes to the redox reaction of ferrocene. It was observed an increase of both the oxidation current and reduction current upon the addition of  $\text{H}_2\text{O}_2$ , which is in accordance with literature report of Fc mediated HRP catalytic reaction toward  $\text{H}_2\text{O}_2$ .<sup>1-3</sup> This result implies that an enzyme-dependent catalytic current response of  $\text{H}_2\text{O}_2$  which originates from the HRP reaction and the soluble redox mediator of ferrocenemethanol could effectively shuttle electrons from the base electrode.

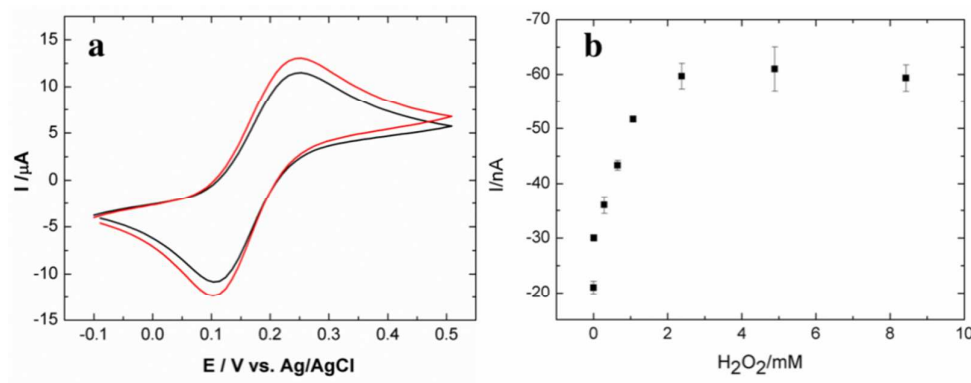
This typical enzyme-dependent catalytic process (shown in Scheme. 1) can be expressed as follows:



First,  $\text{H}_2\text{O}_2$  in the solution is reduced by the immobilized HRP. Then the reduced HRP is regenerated with the aid of the mediator (Fc), while Fc itself is oxidized in the enzymatic reaction. Finally, the oxidized Fc is electrochemically reduced on the electrode, leading to an increase of the reduction current. Since concentration of  $\text{TNF-}\alpha$  influences the immobilized amount of HRP, which is further related to reductive current produced, thus a methodology depends on the relationship between concentration of  $\text{TNF-}\alpha$  and reductive current signal can be developed to monitor  $\text{TNF-}\alpha$ .

Influence of  $\text{H}_2\text{O}_2$  on the response of immunosensor is of great importance, the amperometric response of the mixed layers based immunosensor for  $\text{H}_2\text{O}_2$  reduction was thus examined at an applied potential of 0.05 V upon successive addition of  $\text{H}_2\text{O}_2$  in a gentle stirring PBS containing 0.1 mM ferrocenemethanol. As illustrated in Figure. S-1(b) the immunosensor displays increasing amperometric responses to  $\text{H}_2\text{O}_2$

with the linear ranges from 0.01 mM to 1.07 mM and the maximal cathodic peak current change can be obtained at  $\sim 2.0$  mM  $\text{H}_2\text{O}_2$  and then it started to reach a plateau. In order to avoid the irreversible transition of the HRP to its higher oxidized and inactive form at higher  $\text{H}_2\text{O}_2$  concentration,<sup>4</sup> 2.0 mM of  $\text{H}_2\text{O}_2$  was chosen for following detection.



**Figure S-1.** (a) Cyclic voltammograms of the final immunosensor at 0.1 mM Fc, pH 7.4 PBS in the absence (black line) and presence of 50  $\mu\text{M}$   $\text{H}_2\text{O}_2$  (red line) with a scan rate of 20 mV/s. (b) Dependence of the chronoamperometric reduction current on the concentration of  $\text{H}_2\text{O}_2$  for the PPC-PBA mixed layers-based immunosensor in pH 7.4 PBS containing 0.1 mM Fc at an applied potential of 0.05 V vs. Ag/AgCl. Error bars represent the standard deviation,  $n=3$ .

## References

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