

## Supporting Information

### **Robust Biopolymeric Supramolecular “Host–Guest Macromer” Hydrogels Reinforced by in Situ Formed Multivalent Nanoclusters for Cartilage Regeneration**

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#### **Experimental section**

##### **Preparation of HGM hydrogels and MeHA hydrogels**

Functionalized hyaluronic acids (AD<sub>x</sub>HA or MeHA) were firstly dissolved in PBS (pH=7.4) and then mixed with the photoinitiator I2959 (final concentration: 0.05 wt%). For AD<sub>x</sub>HA, the host monomer mono-Ac- $\beta$ CD (the molar ratio between  $\beta$ CD and AD was always kept as 1:1) was then added into the solution before it was loaded in the homemade molds. After 8 minutes of UV irradiation (7 mW/cm<sup>2</sup>), disk like hydrogel objects were obtained.

##### **In vitro chondrogenesis of hMSCs**

hMSCs (purchased from Lonza) were photoencapsulated (10 million cells/mL) in hydrogels (each hydrogel was fabricated from 50  $\mu$ L precursor solution, loaded with 100 ng TGF- $\beta$ 1), which were cultured in chondrogenic media (DMEM, 1% (vol/vol) ITS+ Premix, 50  $\mu$ g/mL L-proline, 0.1  $\mu$ M dexamethasone, 0.9 mM sodium pyruvate, 50  $\mu$ g/mL ascorbate, and antibiotics) and changed three times per week.

##### **BSA release study**

BSA was mixed with the pre-gelation solution of HGM or MeHA hydrogels for hydrogel preparation as described above (50  $\mu$ g BSA for each hydrogel). The as-prepared hydrogels were then immersed in 1 mL PBS. 50  $\mu$ L PBS from each sample was collected for quantification of the released BSA proteins from the hydrogels. A BCA protein quantification kit was used to quantify the BSA concentration in the medium.

##### **Construct analysis**

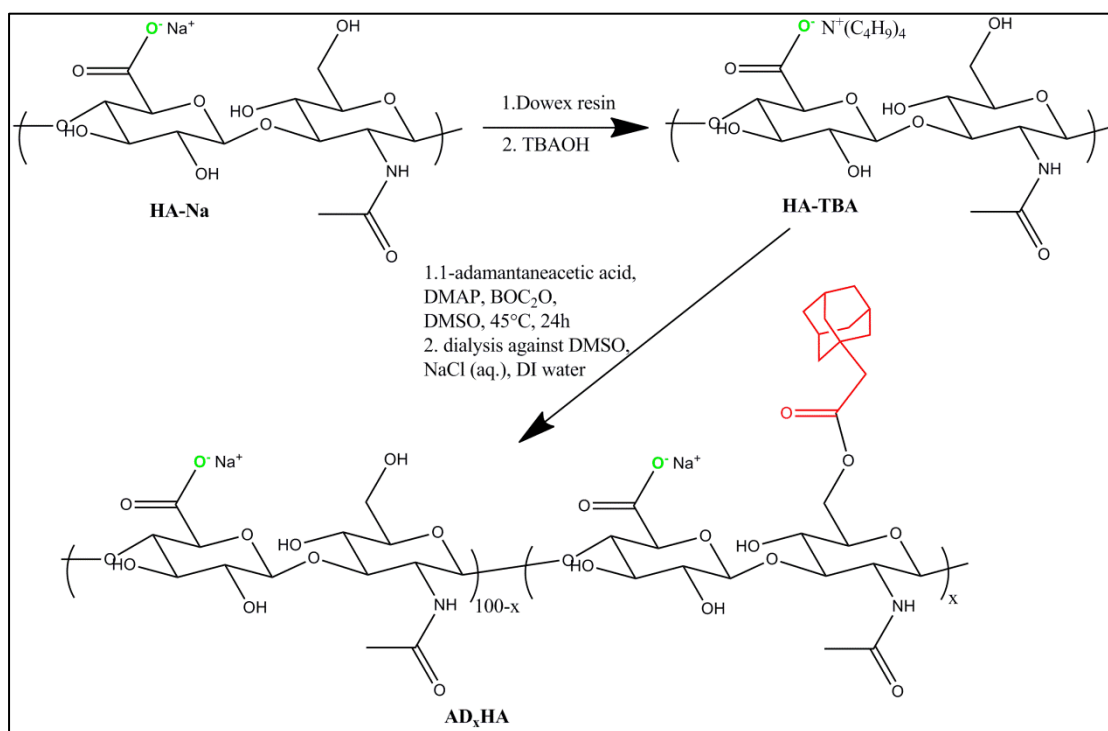
For gene expression analysis, samples were homogenized in TRIzol reagent and RNA

was extracted. After the extracted RNA was reverse-transcribed into cDNA, PCR was performed (primers listed in Table S1). The relative gene expression was calculated using the  $\Delta\Delta C_t$  method, and relative expression was calculated using the expression  $2^{-\Delta\Delta C_t}$ , normalized to GAPDH. For quantification of GAG content, samples were digested in proteinase-K and assessed for GAG content with dimethylmethylene blue. All data are presented as mean  $\pm$  SD. Statistica (Statsoft) was used to perform statistical analysis using two-way ANOVA with Tukey's honestly significant difference post hoc test of the means used to make comparisons between groups (n = 4 samples per group), with experimental group as independent factors.

### Animal study

Hydrogel constructs were made as aforementioned and then sliced to suitable size before implanted in osteochondral defects (d=1mm) in the knees of Sprague-Dawley rats (male, age 8 weeks). All animal procedures were approved and guided by the Institutional Animal Care and Use Committee at the Chinese University of Hong Kong.

### Synthesis and characterization



**Figure S1.** Synthesis of guest polymer  $AD_xHA$ .

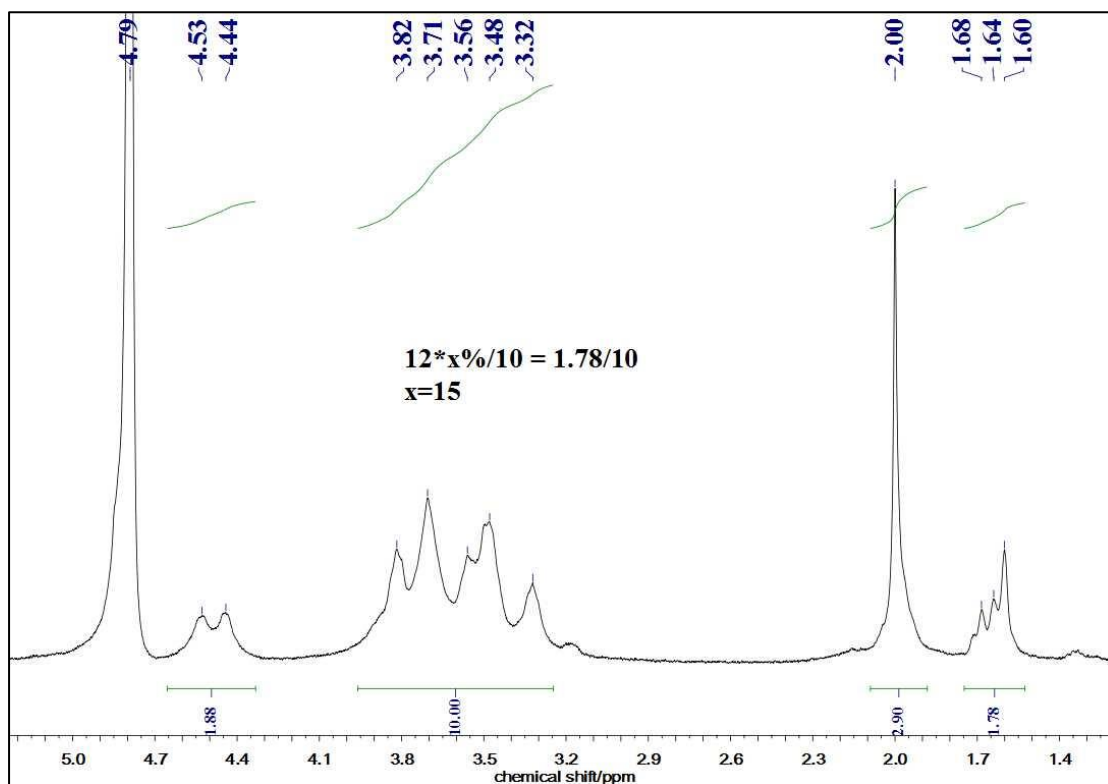


Figure S2. <sup>1</sup>H NMR (D<sub>2</sub>O) of Ad<sub>x</sub>HA, x=15.

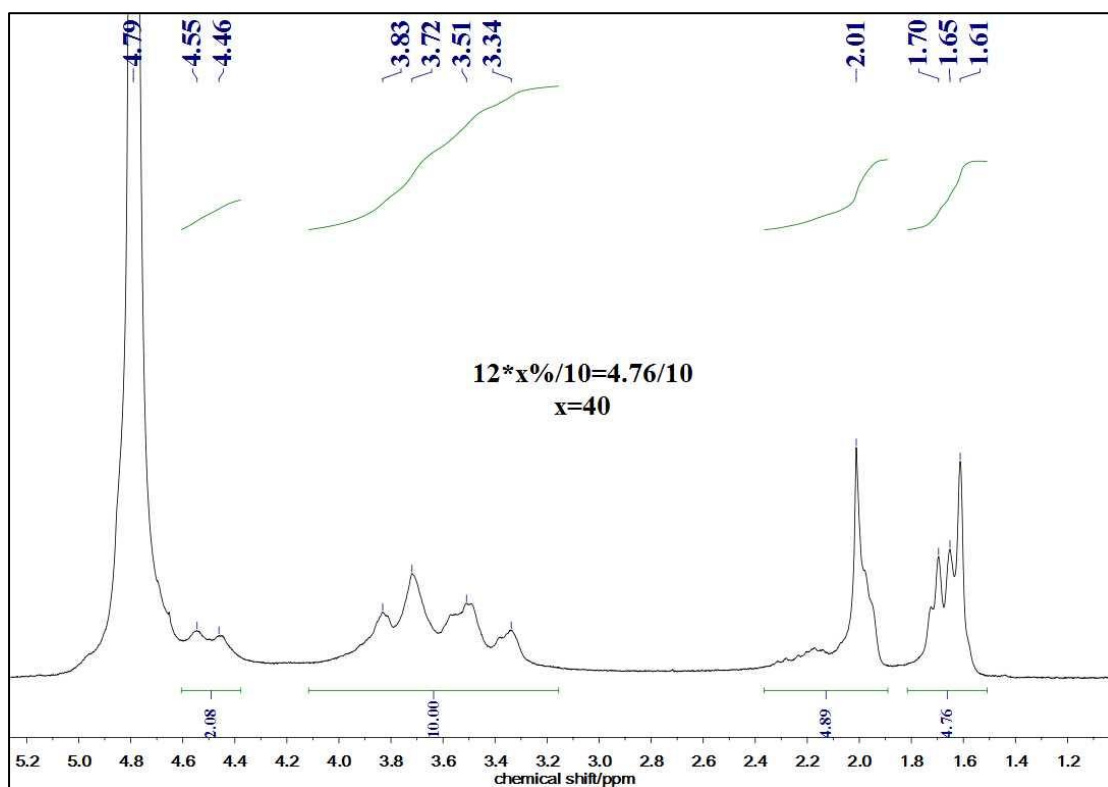
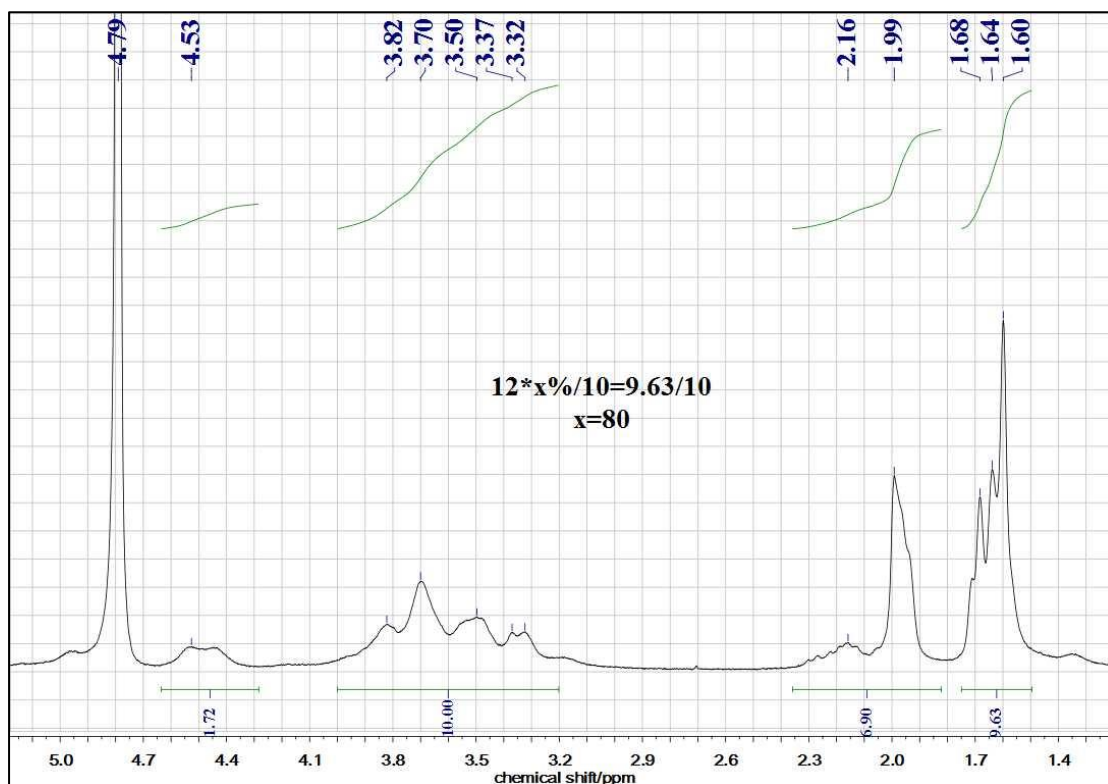
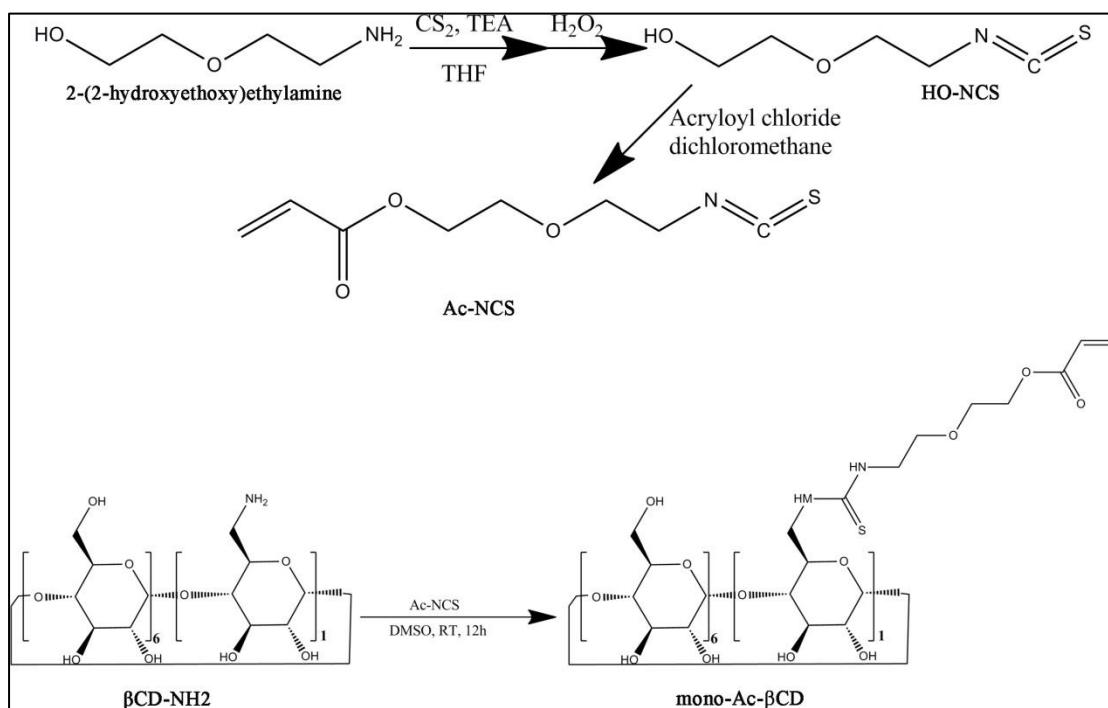


Figure S3. <sup>1</sup>H NMR (D<sub>2</sub>O) of Ad<sub>x</sub>HA, x=40.



**Figure S4.**  $^1\text{H}$  NMR ( $\text{D}_2\text{O}$ ) of  $\text{Ad}_x\text{HA}$ ,  $x=80$ .



**Figure S5.** Synthesis of mono-Ac- $\beta\text{CD}$ .

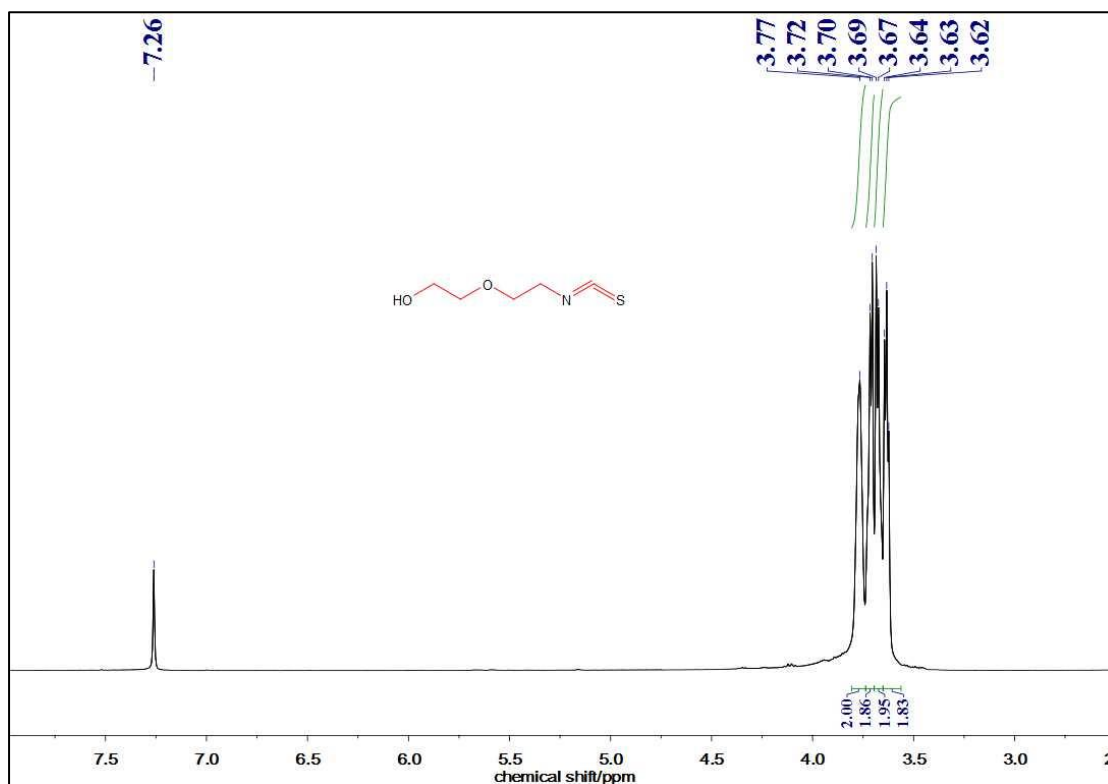


Figure S6.  $^1\text{H}$  NMR ( $\text{CDCl}_3$ ) of HO-NCS.

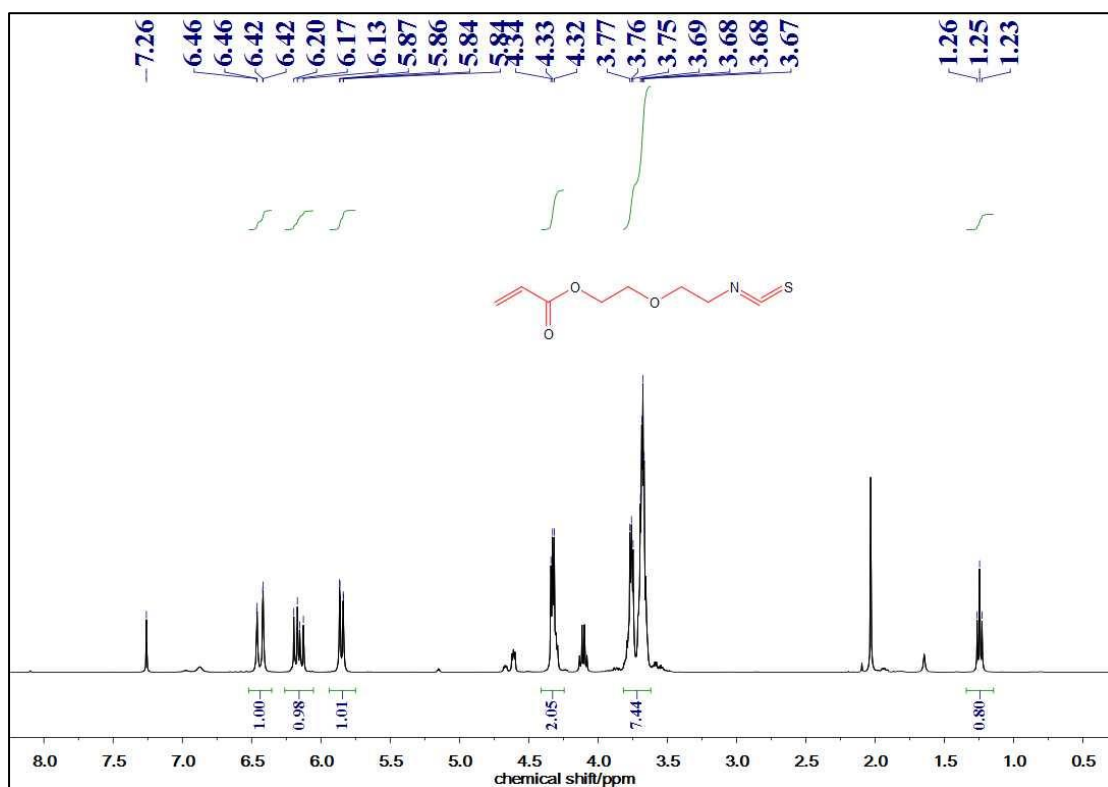
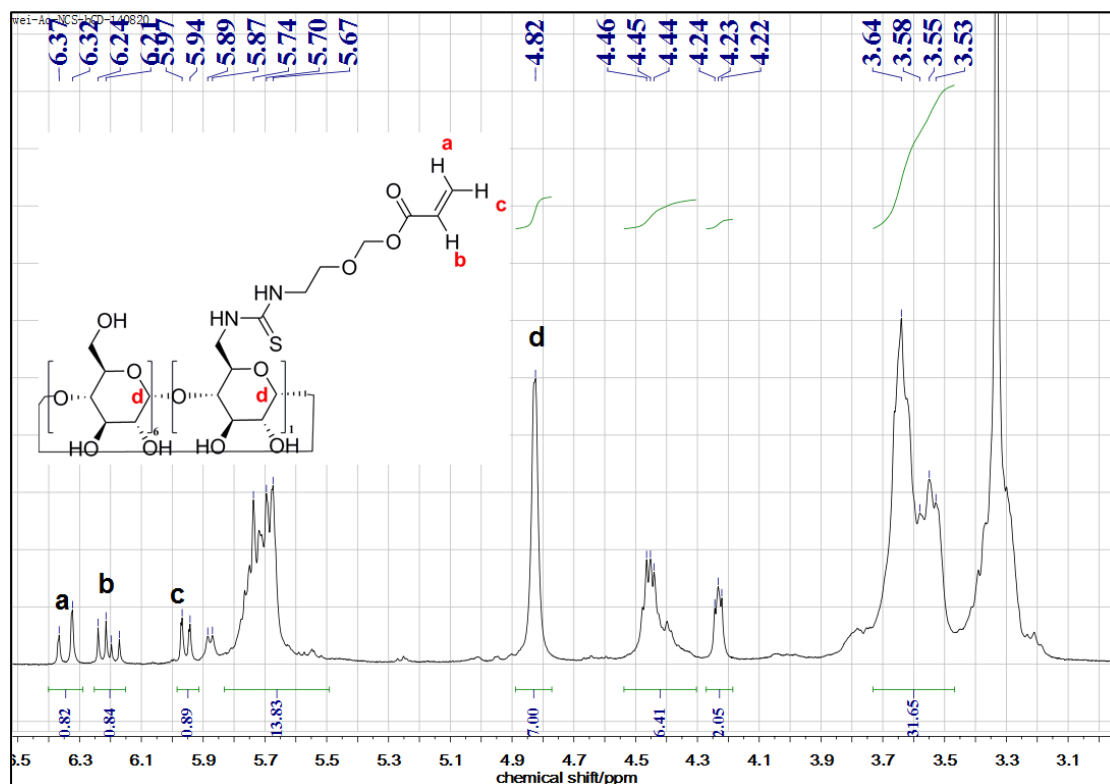
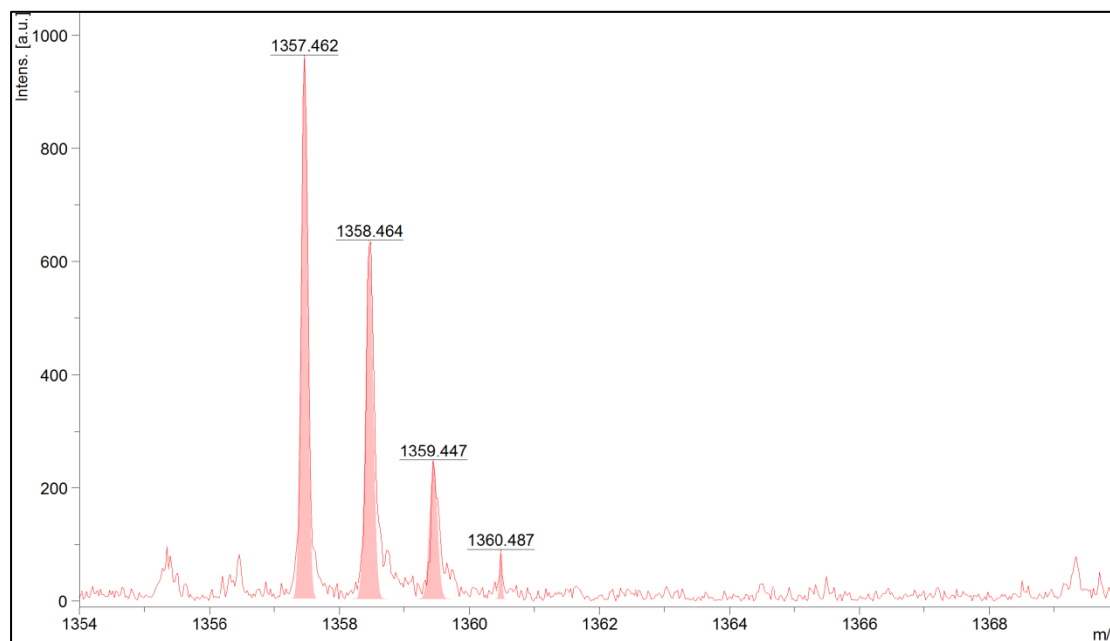


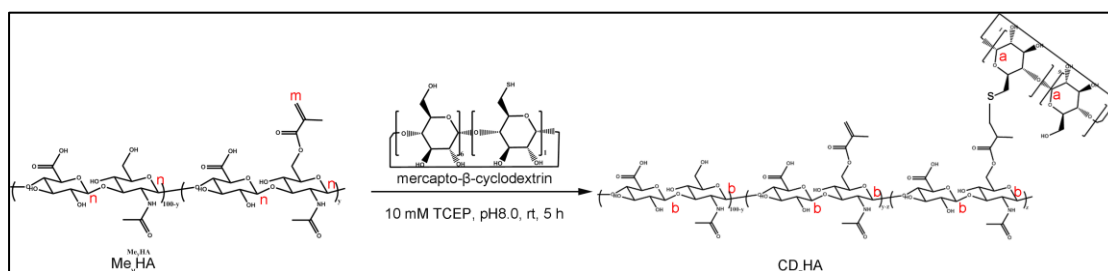
Figure S7.  $^1\text{H}$  NMR ( $\text{CDCl}_3$ ) of Ac-NCS.



**Figure S8.**  $^1\text{H}$  NMR (DMSO- $d_6$ ) of mono-Ac- $\beta$ CD.



**Figure S9.** MALDI-TOF MS of mono-Ac- $\beta$ CD.

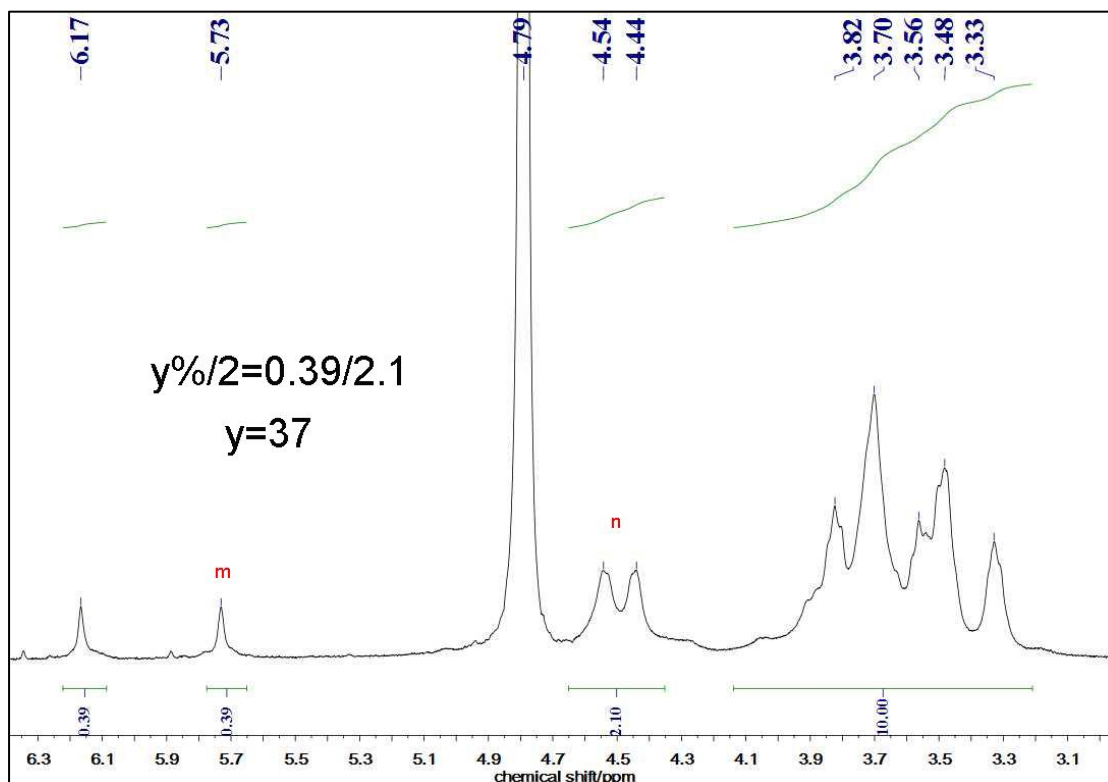


**Figure S10.** Synthesis of host polymer CD<sub>15</sub>HA.

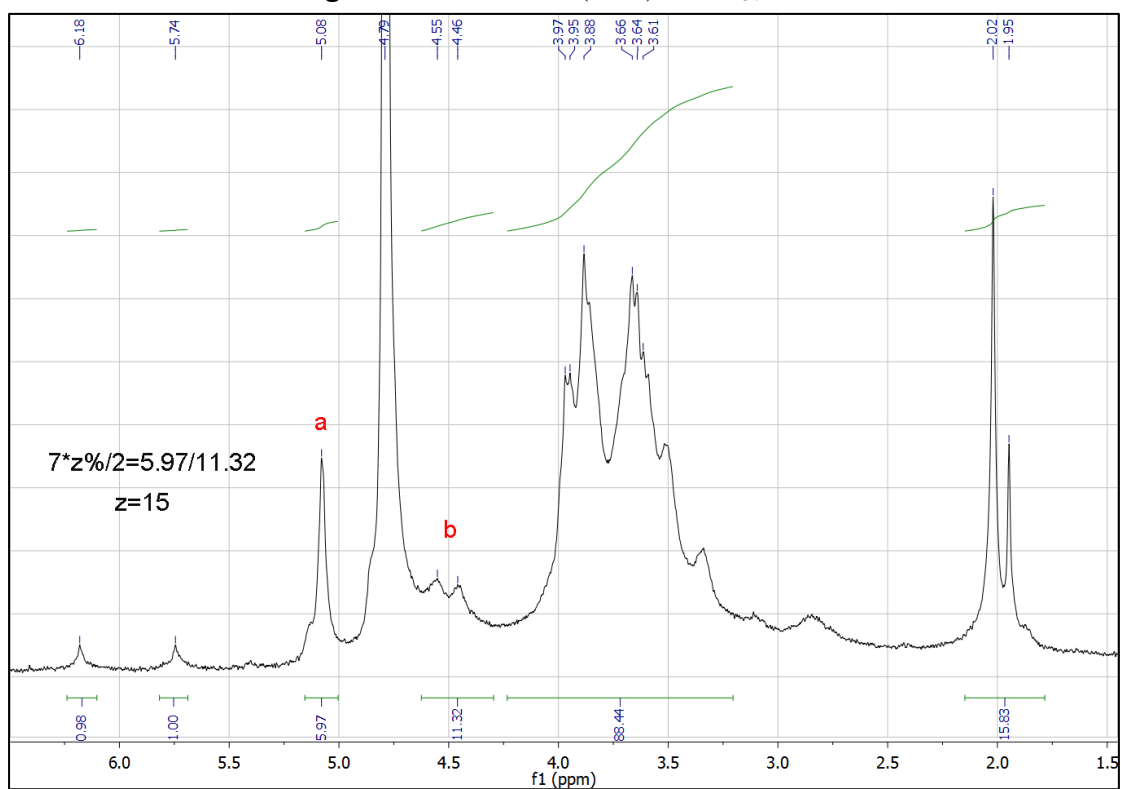
### Methacrylate hyaluronic acid (Me<sub>37</sub>HA) and host polymer CD<sub>15</sub>HA

Methacrylated HA was synthesized according to the previously reported procedure.<sup>1</sup> Briefly, a 20-fold excess of methacrylic anhydride was added to 1% (wt/vol) HA solution in deionized water, pH of the solution was kept around 8, adjusting by 5M NaOH (aq.). After stirring at 5°C for 24h, the product was purified via dialysis against DI water (molecular weight cutoff 6-8 kDa), and then freeze dried. Methacrylation degree of HA was calculated by <sup>1</sup>H NMR integration ratio between protons denoted as *m* and *n* in Figure S10-S11 (y~37%).

Me<sub>37</sub>HA (50 mg) and mercapto-β-cyclodextrin (65 mg) were mixed in 4 mL phosphate buffer (pH 8.0) containing 10 mM tris(2-carboxyethyl)phosphine (TCEP) at room temperature. The mixture was kept on gentle vortex for 5 h, and then dialyzed against water (cutoff Mw. 7000 Da) for one week. After lyophilization, the product was characterized by <sup>1</sup>H NMR and the modification degree was determined by the integration ratio between protons denoted as *a* and *b* in Figure S10 and Figure S12 (z~15%).

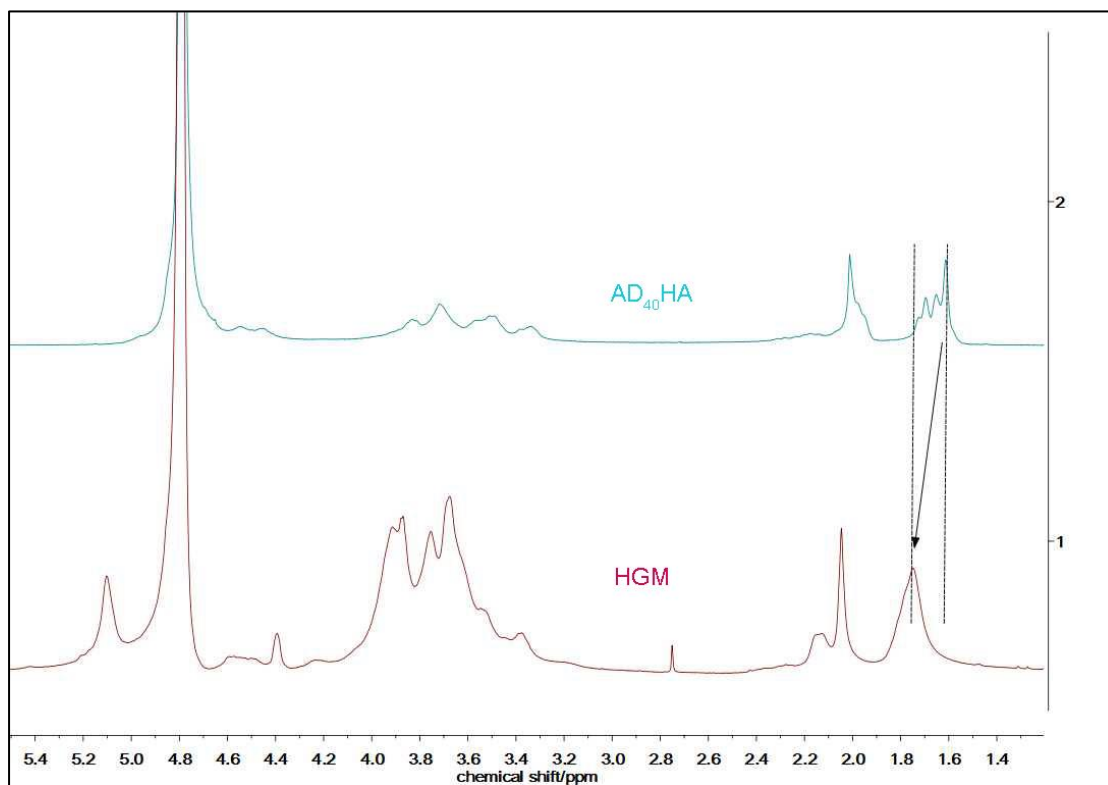


**Figure S11.**  $^1\text{H}$  NMR ( $\text{D}_2\text{O}$ ) of  $\text{Me}_{37}\text{HA}$ .



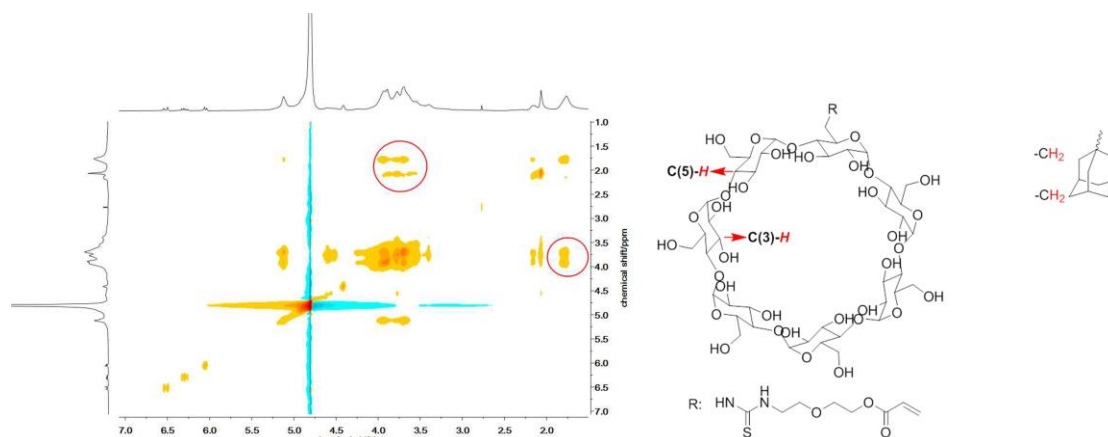
**Figure S12.**  $^1\text{H}$  NMR ( $\text{D}_2\text{O}$ ) of host-polymer  $\text{CD}_{15}\text{HA}$ .

### Characterization of the host-guest-macromer (HGM)



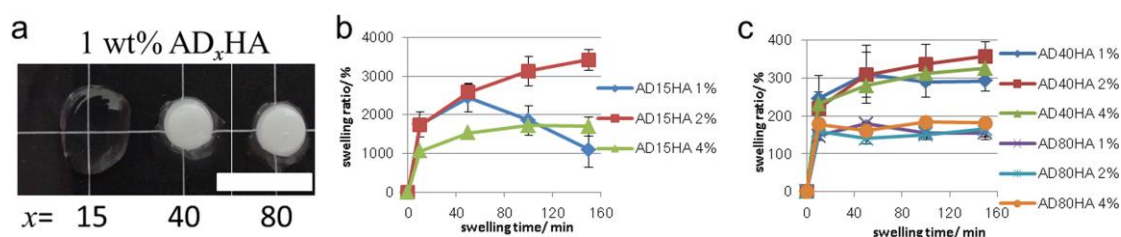
**Figure S13.**  $^1\text{H}$  NMR ( $\text{D}_2\text{O}$ ) of  $\text{AD}_{40}\text{HA}$  and HGM consisting of  $\text{AD}_{40}\text{HA}$  and mono-Ac- $\beta\text{CD}$ . Upon HGM formation, the chemical shift of the ethyl multiplet of AD

changes significantly, and the corresponding peak is broadened.

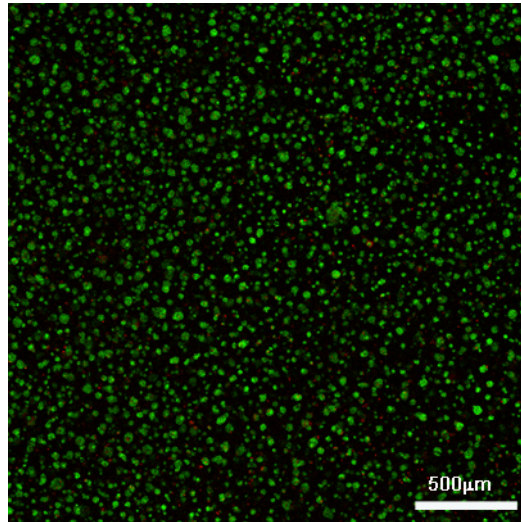


**Figure S14.** 2D NOESY NMR ( $D_2O$ ) of HGM consisting of  $AD_{40}HA$  and mono-Ac- $\beta CD$ , the ADA  $-CH_2$  proton peaks are found correlated with the inner protons (C(3)-H and C(5)-H) of  $\beta CD$ , indicating successful molecular self-assembly between  $AD_{40}HA$  and mono-Ac- $\beta CD$ .

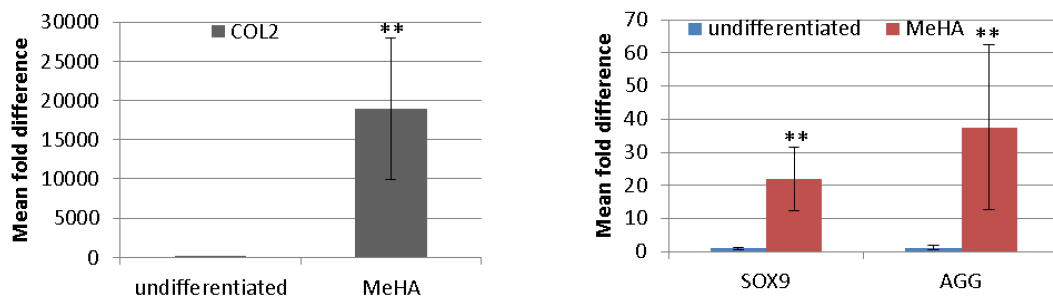
### The swelling behavior of HGM hydrogels



**Figure S15.** Swelling of HGM hydrogels prepared from  $AD_xHA$  of varied concentrations. **(a)** Freestanding HGM hydrogels (1 wt%  $AD_xHA$ ) at equilibrium swollen state (for  $AD_{15}HA$  HGM hydrogels, the equilibrium state is considered at the swelling time of 50min, as shown in panel **(b)**, scale bar: 1 cm); **(b)** swelling kinetics of  $AD_{15}HA$  HGM hydrogels, showing that the hydrogel made from 1 wt%  $AD_{15}HA$  is not stable after 50min of swelling; **(c)** Identical swelling kinetics of HGM hydrogels composed of  $AD_xHA$  with the same modification degree indicates that the modification degree of AD dictates the inter-crosslink polymer chain length, thereby confirming the crosslinking function of AD in the hydrogel networks.



**Figure S16.** Viability staining of the hMSCs encapsulated in the re-molded HGM hydrogels obtained 24 hours after the remolding procedure (Green: living cells; red: dead cells).



**Figure S17.** Gene expression level of COL2 (a), SOX9 and AGG (b) in MeHA hydrogels after 7 days of culture (in chondrogenic media (DMEM, 1% (vol/vol) ITS+ Premix, 50  $\mu$ g/mL L-proline, 0.1  $\mu$ M dexamethasone, 0.9 mM sodium pyruvate, 50  $\mu$ g/mL ascorbate, and antibiotics) supplemented with 10 ng/mL TGF- $\beta$ 1 and changed three times per week.).

**Table S1. Sequences of primers and probes used for real-time PCR**

Gene	Forward primer	Reverse primer	probe
COL2	GGCAATAGCAGGTTACGTACA	CGATAACAGTCTTGCCCCACTT	CTGCACGAAACATAC
GAPDH	AGGGCTGCTTTTAACTCTGGTAAA	GAATTGCCATGGGTGGAAT	CCTCAACTACATGGTTTAC
SOX9	AAGCTCTGGAGACTTCTGAACGA	GCCCCGTTCTTCACCGACTT	CCGGATTACAAGTACCAGC
AGG	TCGAGGACAGCGAGGCC	TCGAGGGTGTAGCGTGTAGAGA	ATGGAACACGATGCCTTTCACCACGA

## Reference

(1) Smeds K. A.; Grinstaff M. W.; *J. Biomed. Mater. Res.* **2001**, *54*, 115-121.