

Supporting Information for

Selective Manipulation of Biomolecules with Insulator-Based Dielectrophoretic Tweezers

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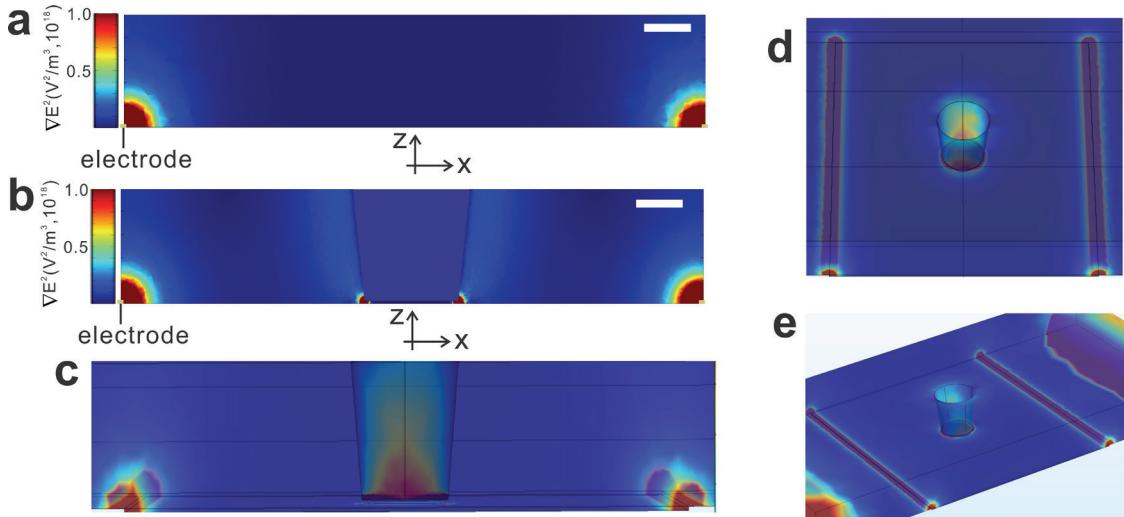


Figure S1. The distribution of ∇E^2 calculated by COMSOL simulation. (a) Localized ∇E^2 at the both electrode under AC voltage V_{ac} ($7\text{ V}_{pp}, f = 50\text{ kHz}$). The scale bar is $5\text{ }\mu\text{m}$. (b) Distribution of the additional localized ∇E^2 at the tip. (c) Cross sectional view of ∇E^2 distribution. (e) Top and (e) side view of ∇E^2 distribution.

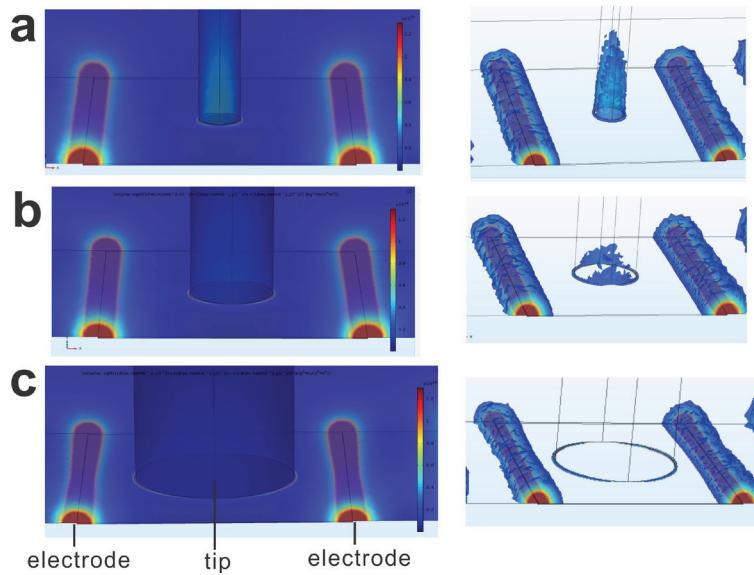


Figure S2. The distribution of ∇E^2 around the tip with its diameter of (a) $4\text{ }\mu\text{m}$ (b) $5\text{ }\mu\text{m}$, and (c) $15\text{ }\mu\text{m}$. For the small tip, the concentrated field at the tip is proportional to the area of the tip (πr^2). In contrast, the field partially interacts with the large tip. Thus, about a quarter of rim contacts with each electrode, and the effective trapping volume is proportional to the circumference of the tip (πr). Our experiments show that the tip diameter of $4 \sim 8\text{ }\mu\text{m}$ offers the most effective trapping of the particles and DNA in our devices.

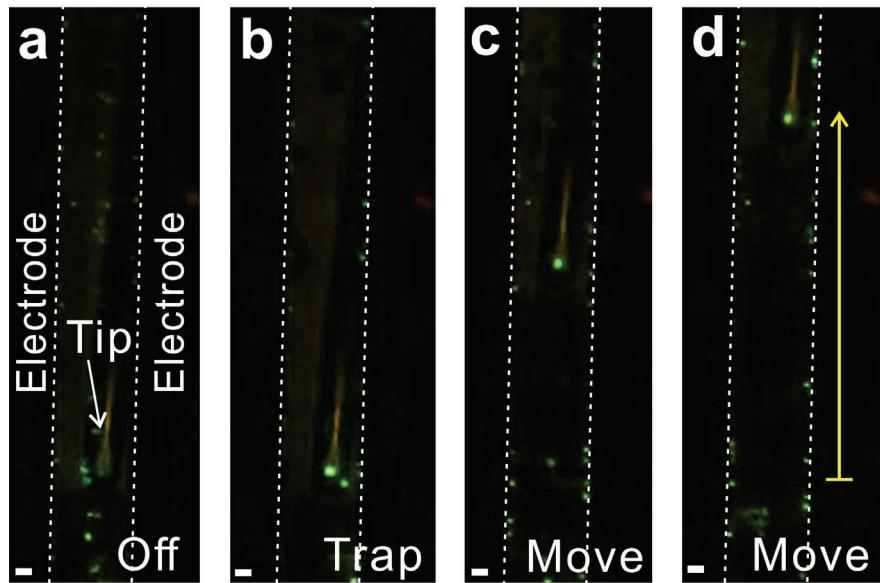


Figure S3. Additional example of nanoparticle manipulation. (a) No AC bias. (b) – (d) Trapping and repositioning of the particles at the tip with the pDEP bias (5 V, 20 kHz). The yellow arrow is 112 μm . The scalar bar is 5 μm .

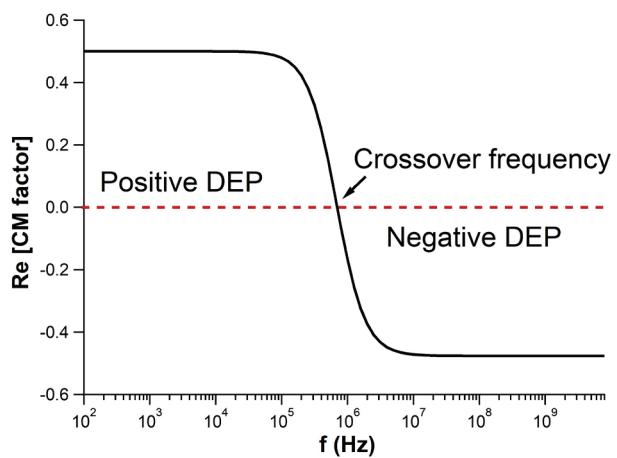


Figure S4. Real part of the CM factor of the spherical particle. In calculating this plot, the following parameters were used: $\epsilon_p = 2.5 \epsilon_0$, $\epsilon_m = 78 \epsilon_0$, $\sigma_p = 4 \times 10^{-3} \text{ S/m}$, $\sigma_m = 1 \times 10^{-3} \text{ S/m}$.

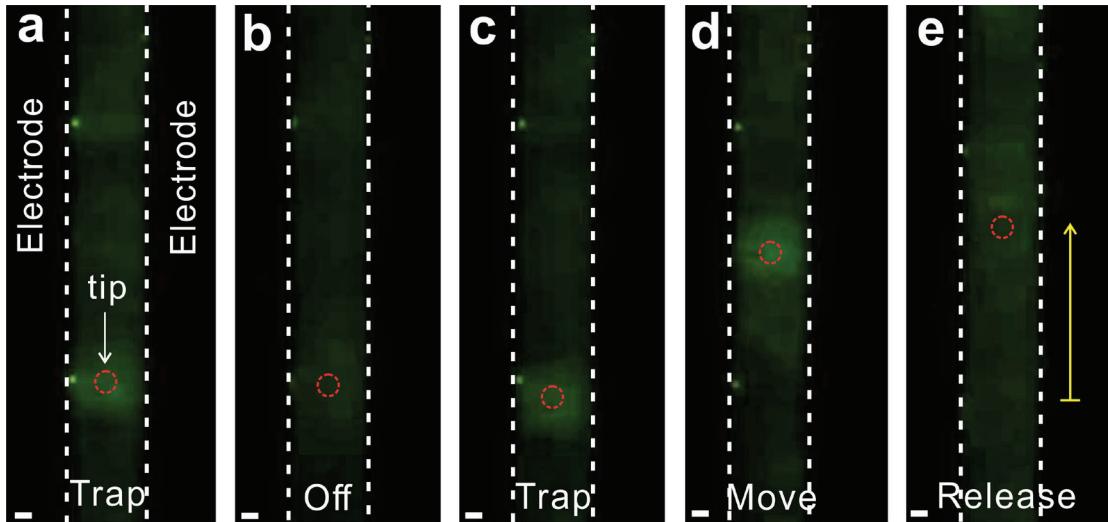


Figure S5. Additional example of homogeneous (48,502 base pairs) DNA manipulation under the pDEP bias ($7 \text{ V}_{\text{pp}}, f = 200 \text{ kHz}$). (a) Tapping, (b) releasing, (c) re-trapping, (d) repositioning, and (e) releasing of DNA at the tip (the red circle). The yellow arrow is $56 \mu\text{m}$. The scalar bar is $5 \mu\text{m}$.

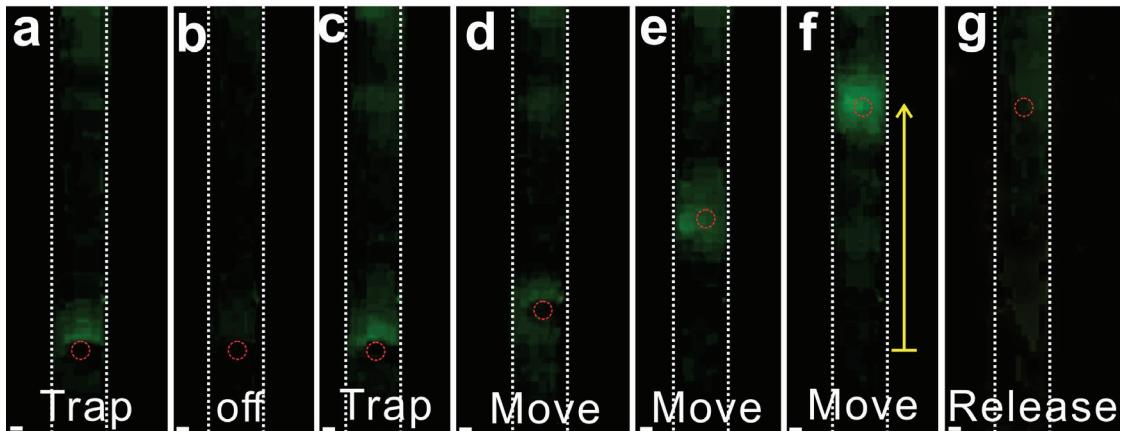


Figure S6. Spatial manipulation of nonhomogeneous mixed DNA containing 6 fragments from $3,550 - 21,226$ base pairs under the pDEP bias ($7 \text{ V}_{\text{pp}}, f = 200 \text{ kHz}$). (a) Tapping and (b) releasing of DNA at the tip (the red circle). (c)-(f) The motion of the tip with trapped DNA along the y-axis. The yellow arrow is $100 \mu\text{m}$. (g) Instant release of DNA at the tip by turning off the trap bias. The scalar bar is $5 \mu\text{m}$.

Estimation of various forces acting on a particle in a fluid environment

We have calculated the magnitudes of various forces including electric thermo flow force, resistive drag, gravity, and buoyancy acting on a moving object in a fluid and compared to iDEP. We have used the DNA ($R = 600$ nm) and velocity of 1 mm/s, which are comparable to our experimental conditions.

First, we estimated gravitational force acting on DNA, $F_g = mg = 5 \times 10^{-19}$ N, which is negligible compared to iDEP estimated by the CM factor model (18 nN and 41.5 nN) in the main text.

Second, buoyant force can be calculated by $F_B = \rho g V$, where ρ is the density of the buffer (water), and $V = 4\pi r^3/3$ is the volume of DNA in the spherical model in buffer. F_B in this assumption is 2.8×10^{-15} N, which is not comparable to iDEP.

Third, we estimated drag force by $F_{drag} = 0.5 C_d \rho A v^2 + 6\pi\eta rv$, where C_d is drag coefficient ranging from 0.1 to 1, A is the cross section of an object moving in liquid, v is the velocity of an object, and η is viscosity¹⁻². The drag force is estimated to be 1.02×10^{-11} N, which is less than 1 % of iDEP.

Finally, we estimated the electric thermo flow force induced by applying AC voltage between two parallel electrodes. The time average force acting on a unit volume is described by, $\langle f \rangle = -M(\omega, T) \left(\frac{\varepsilon \sigma V_{rms}^4}{2k\pi^3 r^3 T} \right) \left(1 - \frac{2\theta}{\pi} \right)$, where M is a dimensionless factor depending on applied frequency with its value $|M| < 7$ at the frequency less than 1 MHz³. Here, ε is permittivity, σ is conductivity, k is thermal conductivity, and T is temperature. θ and r are cylindrical coordinates, respectively, and the origin is located at the middle of two parallel electrodes. We calculated the maximum force by using the maximum of $M(\omega, T) \sim 6.5$ and $\theta = 0$. At $r = 10$ μm , the maximum value of electro thermal fluid force is estimated as $\langle f \rangle_{max} \sim 6.5 \left(\frac{\varepsilon \sigma V_{rms}^4}{2k\pi^3 r^3 T} \right) = 9.65 \times 10^{-17} \text{ N}/\mu\text{m}^3$, which is not comparable to iDEP.

Taken together, our iDEP tweezers enable us to spatially manipulate objects in a fluid, and therefore, our DNA manipulation experiments with iDEP are justified.

References

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- (3) Ramos, A.; Morgan, H.; Green, N. G.; Castellanos, A. Ac electrokinetics: a review of forces in microelectrode structures. *J. Phys. D Appl. Phys.* **1998**, *31* (18), 2338.